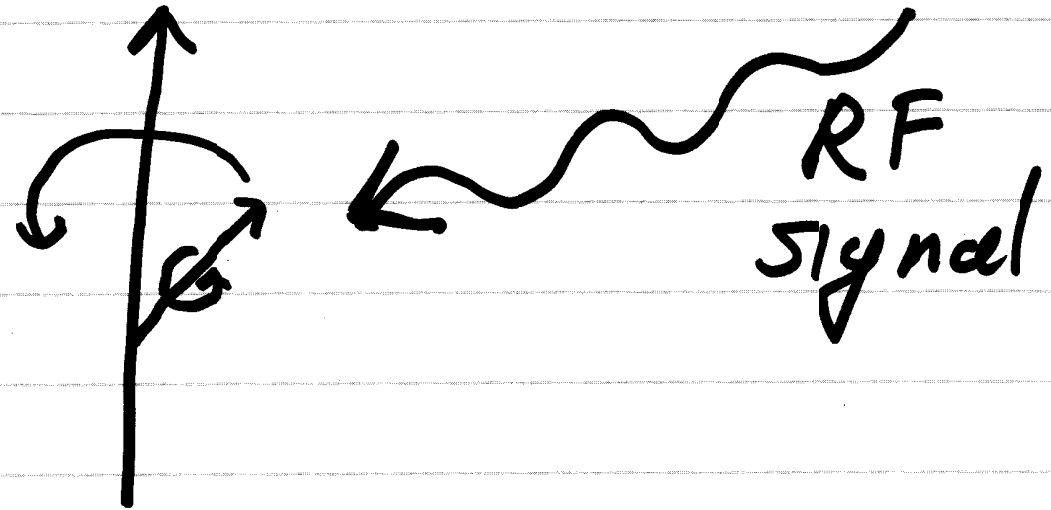


Magnetic Resonance Imaging

- Based on magnetic resonance effect in hydrogen
- Does not require any ionizing radiation
- Numerous modality
 - Functional MRI
 - MRI Tagging
 - high speed MRI

Magnetic Resonance



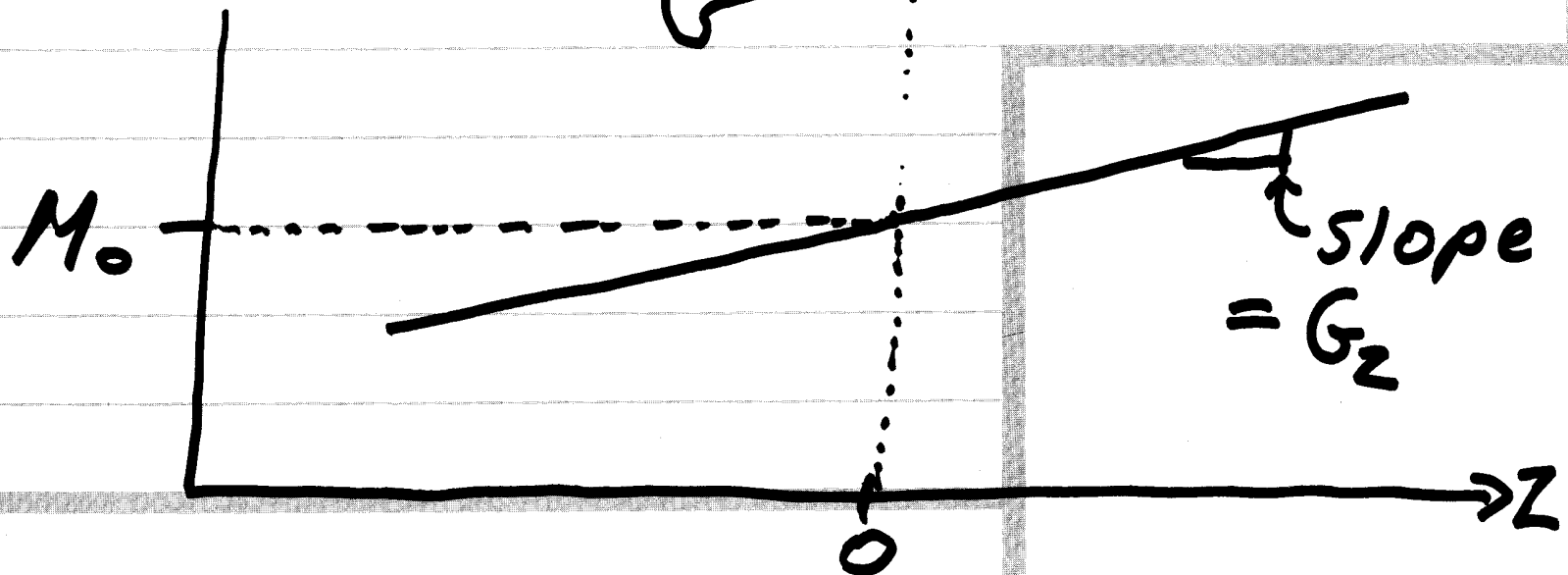
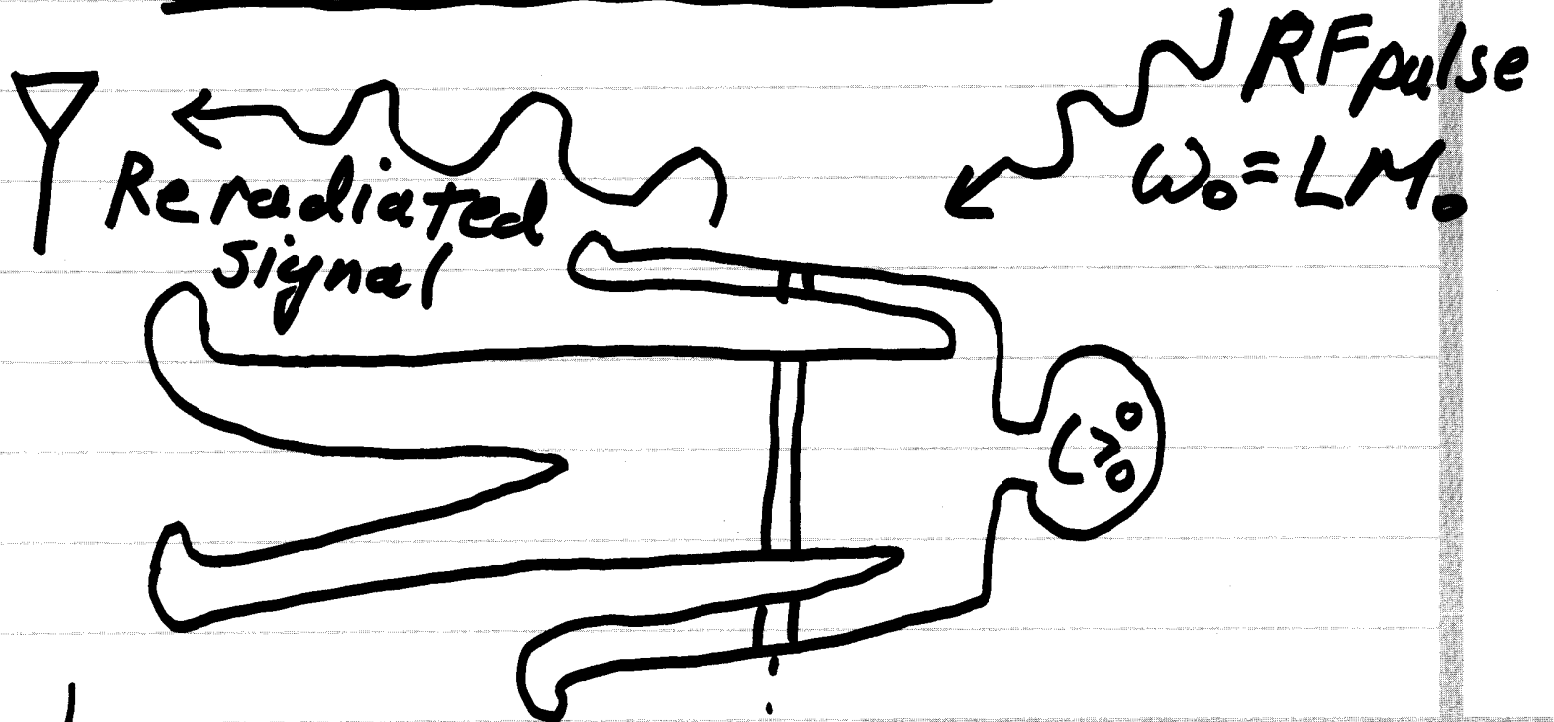
M_0 Magnetic Field

- Atom will process at frequency

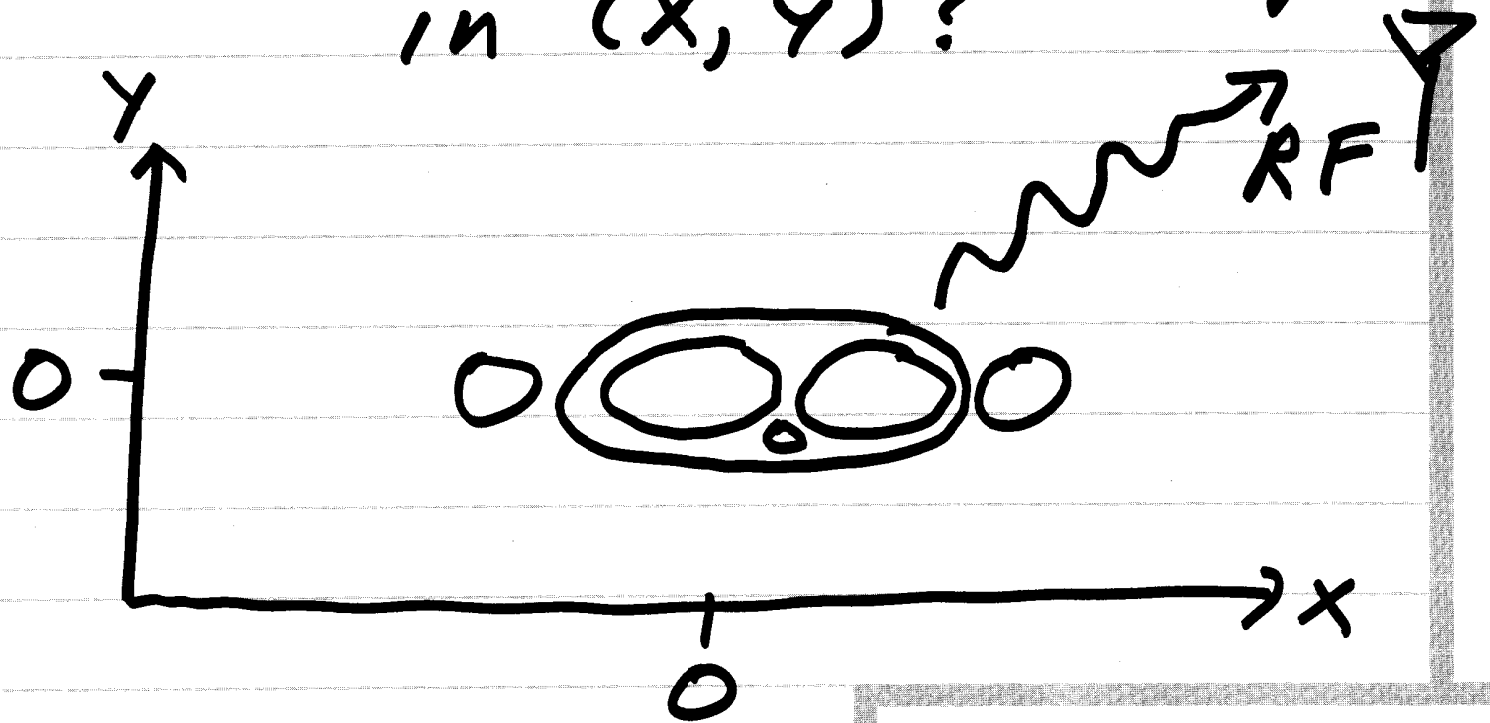
$$\omega_0 = \gamma M_0$$

$\uparrow$ Larmor Frequency

Slice Select



How Do We Form an Image
in (x, y) ?



- Vary magnetic field gradients
in x and y after slice select.

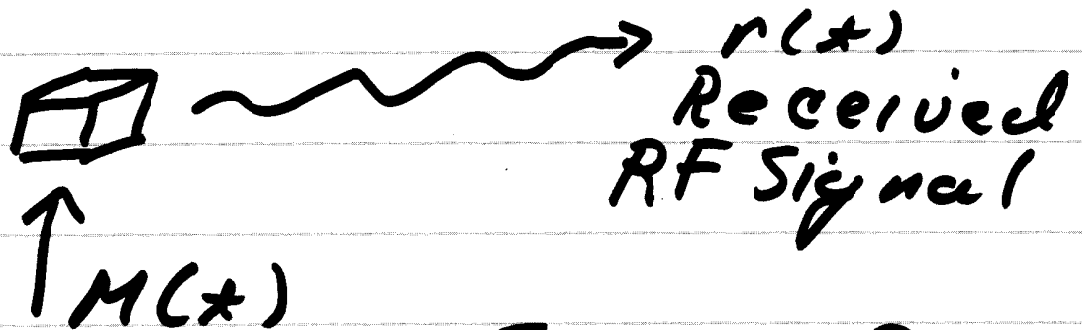
$G_x(x) \leftarrow$ Gradient in X
direction

$G_y(x) \leftarrow$ Gradient in Y
direction

• Total magnetic field

$$M(x) = M_0 + x G_x(x) + y G_y(x)$$

Signal Radiated from a Single Voxel



$$r(x) = f(x, y) \exp\{j\phi(x)\}$$

- $f(x, y)$ is weighting of signal due to material properties.
 - Typically $T1$, $T2$, or $T2^*$ weighted.
- $\phi(x)$ is phase of signal

$$\phi(t) = \int_0^t \{ L M_0 + L x G_x(\tau) + L y G_y(\tau) \} d\tau$$

$$= t \underbrace{L M_0}_{\omega_0} + x \underbrace{\int_0^t L G_x(\tau) d\tau}_{K_x(t)} + y \underbrace{\int_0^t L G_y(\tau) d\tau}_{K_y(t)}$$

Define

K-space

$$\begin{cases} K_x(t) \triangleq \int_0^t L G_x(\tau) d\tau \\ K_y(t) \triangleq \int_0^t L G_y(\tau) d\tau \end{cases}$$

Instantaneous Frequency

$$\text{Instantaneous Freq.} = \frac{d\phi(t)}{dt}$$

$$= \angle M(t) = \angle \text{amplitude Freq.}$$

$$\phi(t) = \int_0^t \angle M(\tau) d\tau$$

$$M(t) = M_0 + x G_x(t) + y G_y(t)$$

$$\phi(t) = t\omega_0 + x k_x(t) + y k_y(t)$$

$$r(t) = f(x, y) e^{j\omega_0 t} \cdot e^{j(x k_x(t) + y k_y(t))}$$

↑
signal radiated from
a single voxel



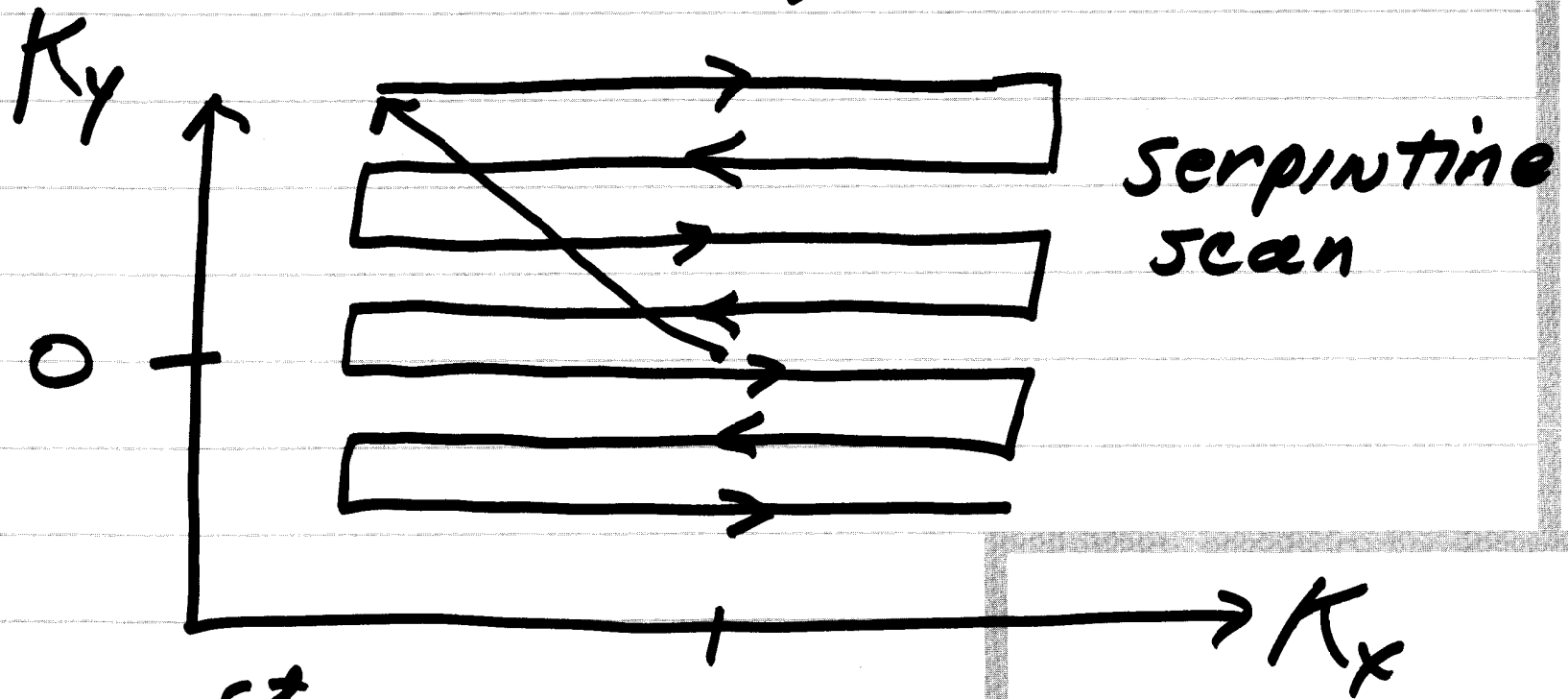
Signal Radiated From Selected Slice

$$R(t) = \iint_{\mathbb{R}^2} f(x, y) e^{j\omega_0 t} e^{j(xk_x(t) + yk_y(t))} dx dy$$
$$= e^{j\omega_0 t}.$$

$$\int_{\mathbb{R}^2} f(x, y) e^{j(xk_x(t) + yk_y(t))} dx dy$$

~~DSFT!!~~
(inverse) CSFT!!

Echo Planar Imaging (EPI)



$$k_x = \int_0^T \gamma G_x(\tau) d\tau$$

$$k_y = \int_0^T \gamma G_y(\tau) d\tau$$

Gradient Wave forms of EPI

